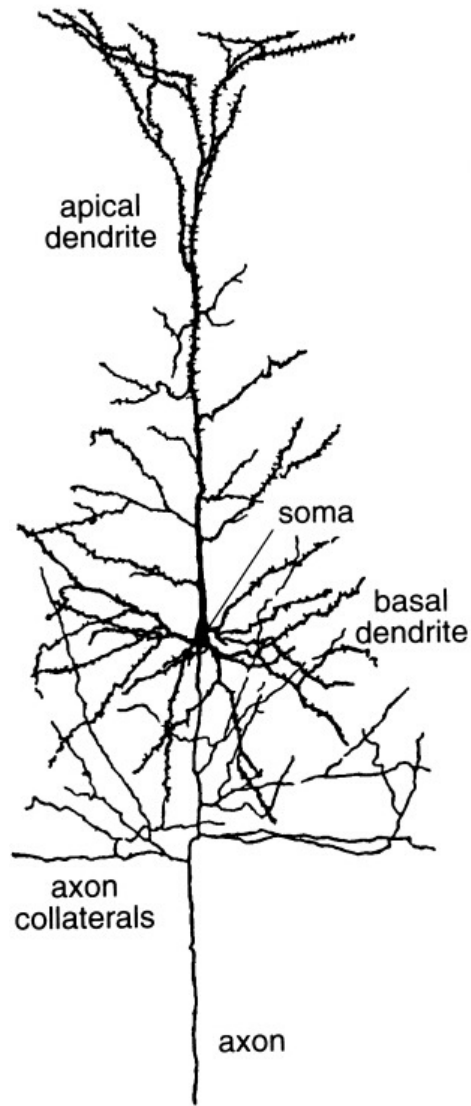
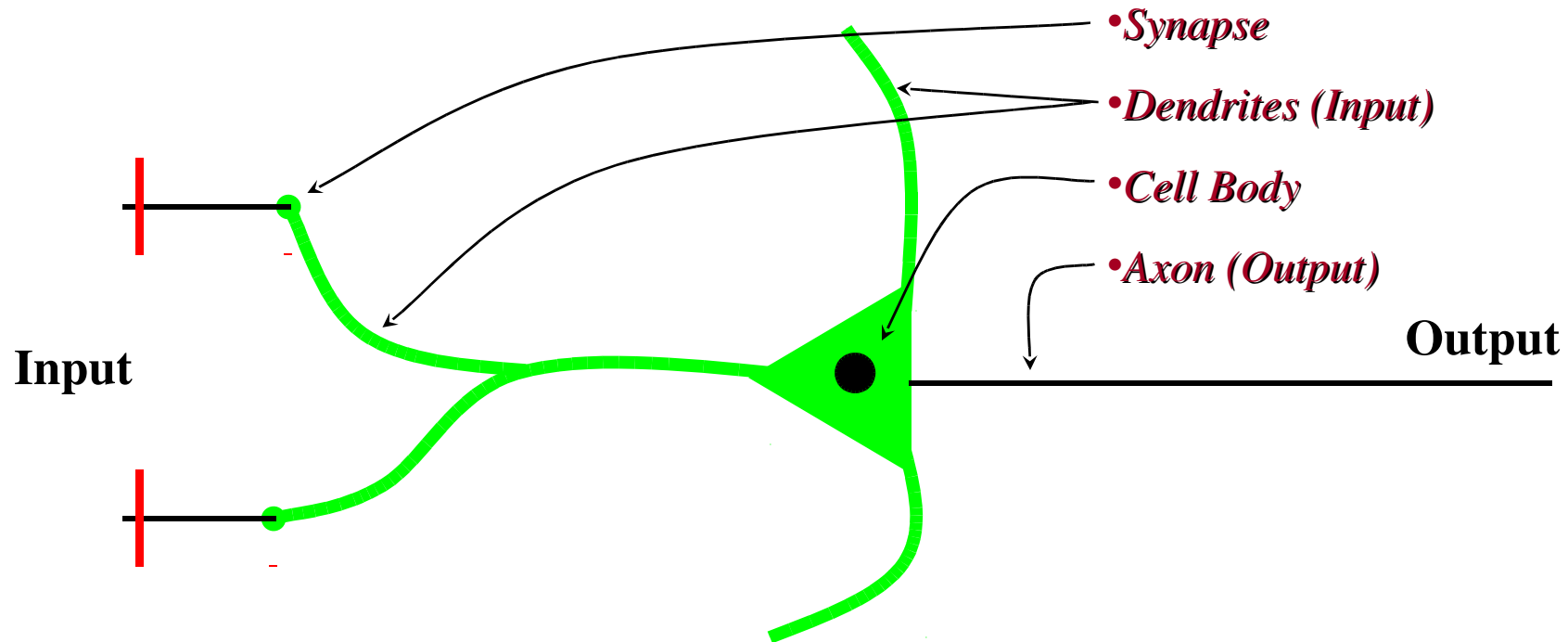


Neuroelectronics

The Neuron



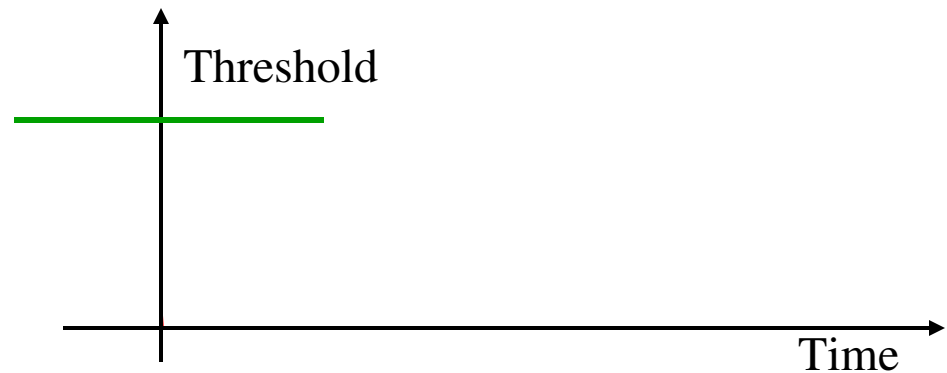
Neuron: The Device



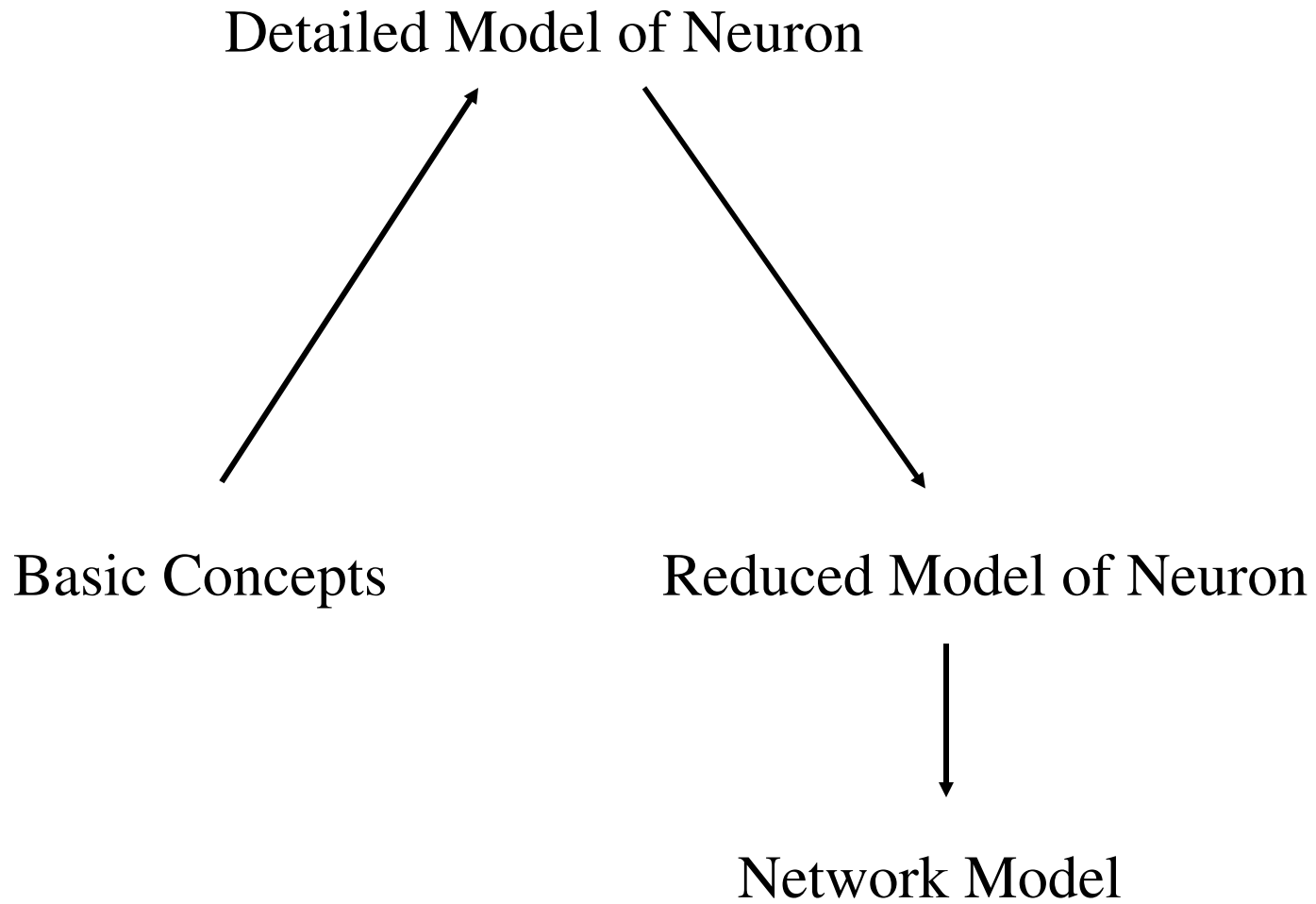
Equilibrium: Membrane Potential

Dendrites: Passive Conductance

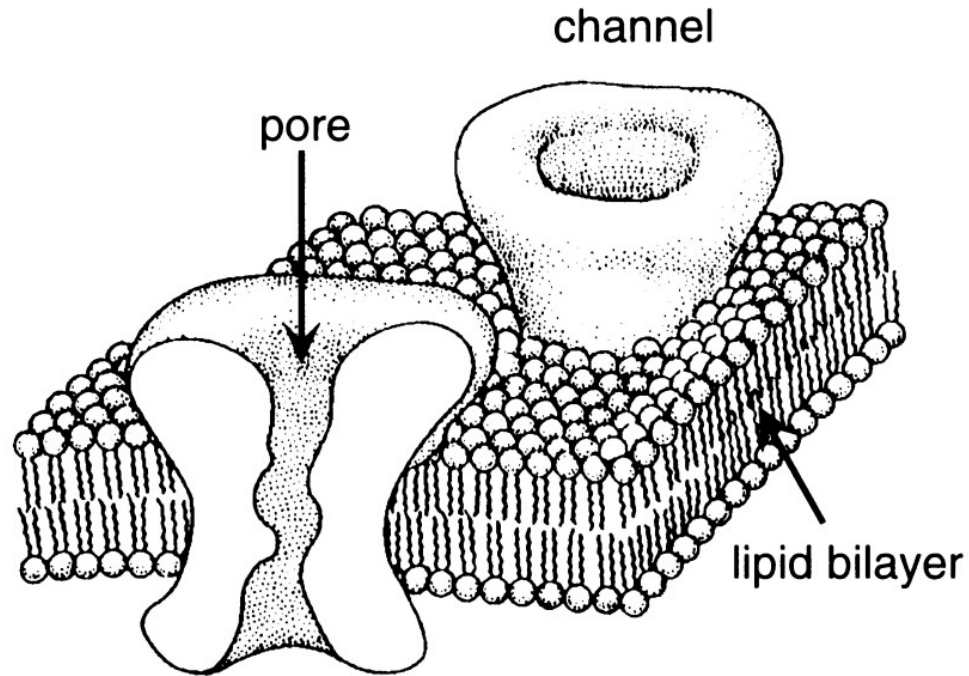
Axon: Spikes (Hodgkin Huxley Eqns)



Approach



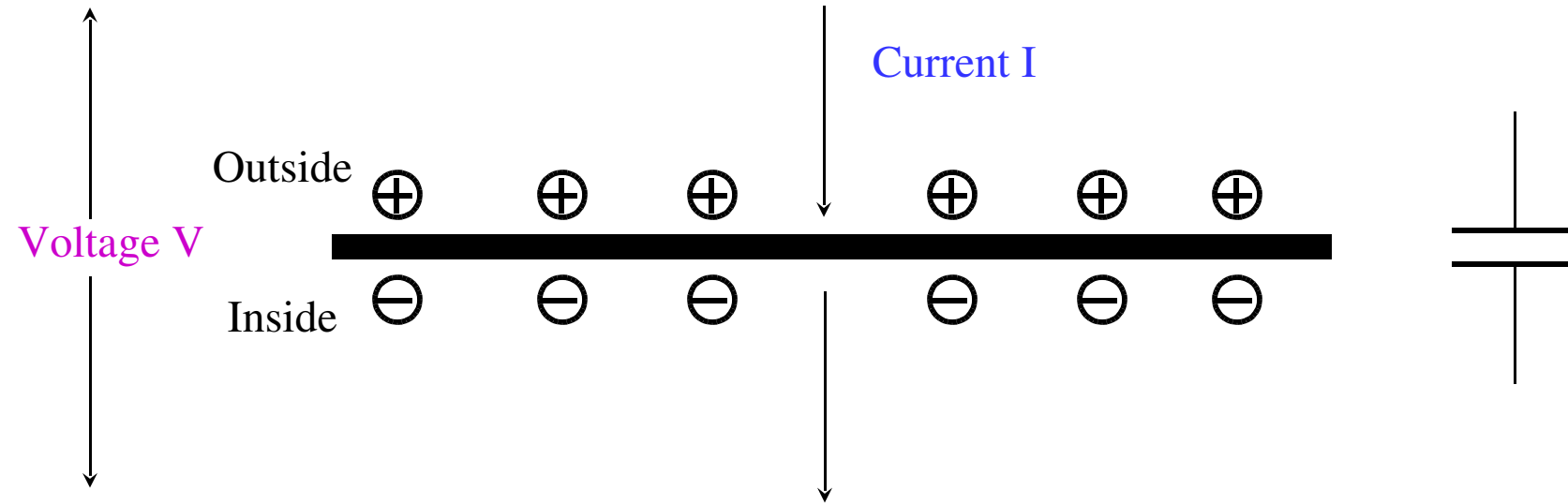
The Membrane



Membrane: 3 to 4 nm thick, essentially impermeable

Ionic Channels: Selectively permeable (10,000 times smaller resistance)

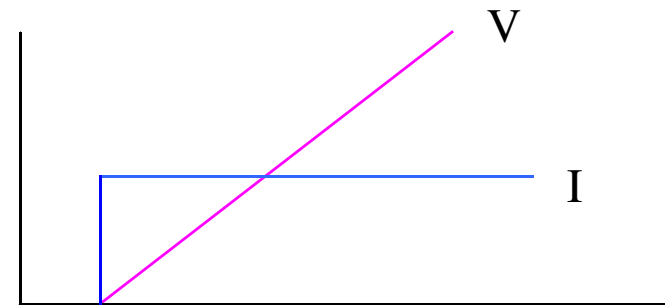
The Membrane: Capacitance



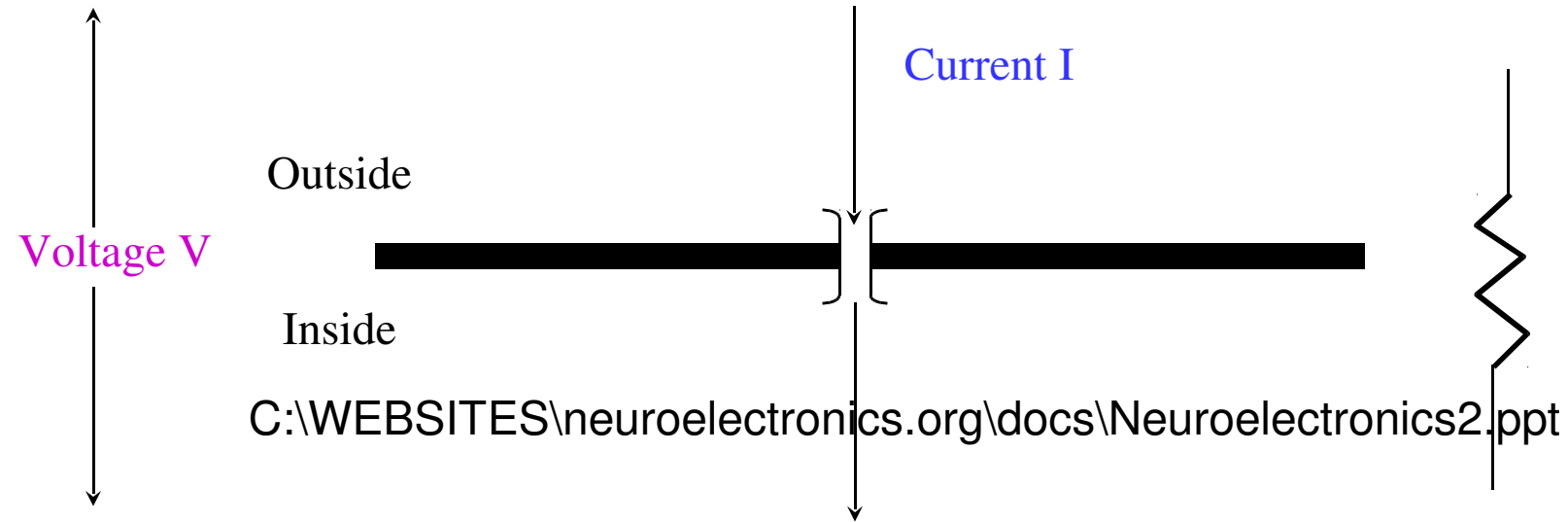
$$C = Q/V \quad 1 \text{ Farad} = 1 \text{ Coulomb} / 1 \text{ Volt}$$
$$(Q = CV);$$

$$dQ/dt = I$$

$$I = C dV/dt$$

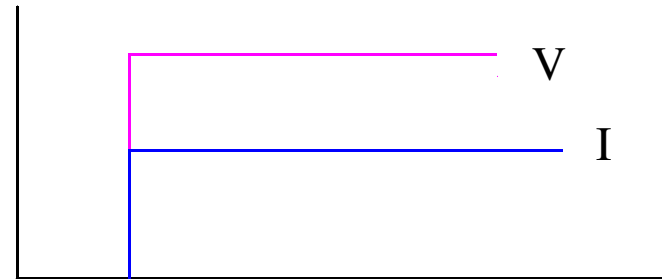


The Membrane: Resistance

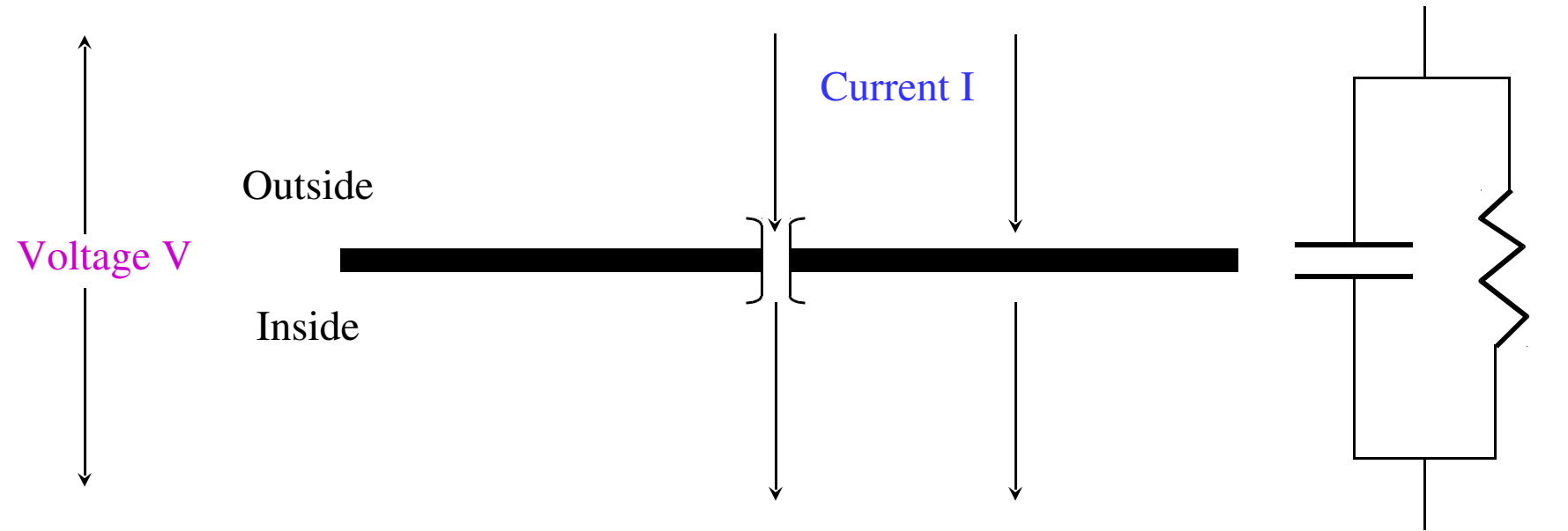


$$R = V/I \quad 1 \text{ Ohm} = 1 \text{ Volt} / 1 \text{ Ampere}$$

$$I = V/R$$

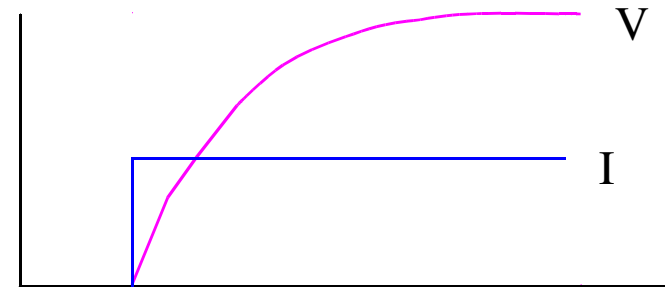


The Membrane: Capacitance and Resistance



$$I = C \frac{dV}{dt} + \frac{V}{R}$$

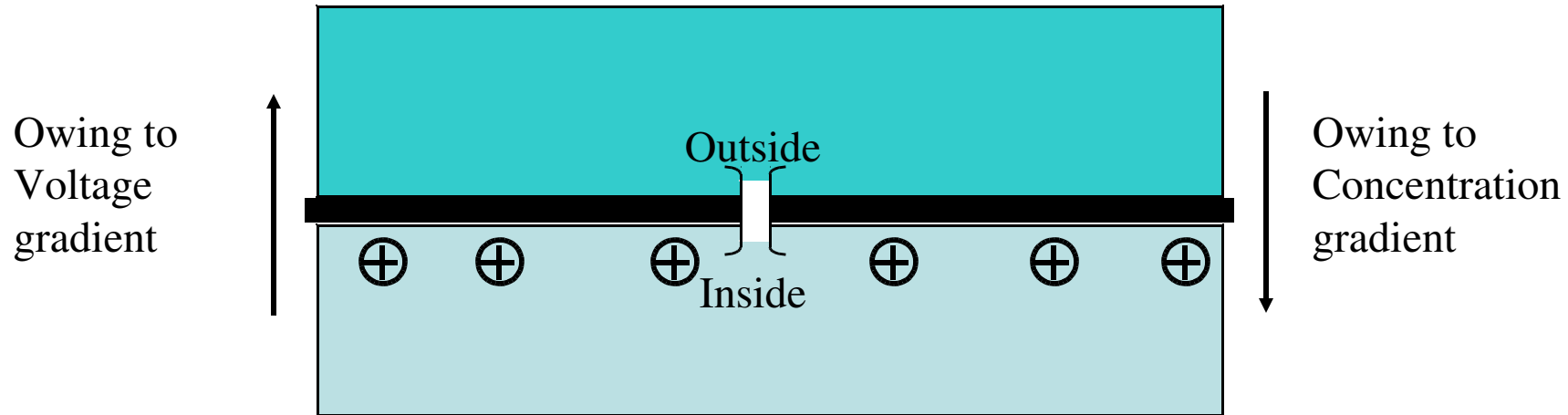
$$(C \cdot R) \frac{dV}{dt} = -V + IR$$



The Membrane: Membrane Potential

Case 1: Single type of Ion (Na^+)

Charge Balanced out by impermeable ion



Reversal Potential : When opposing currents balance each other out.

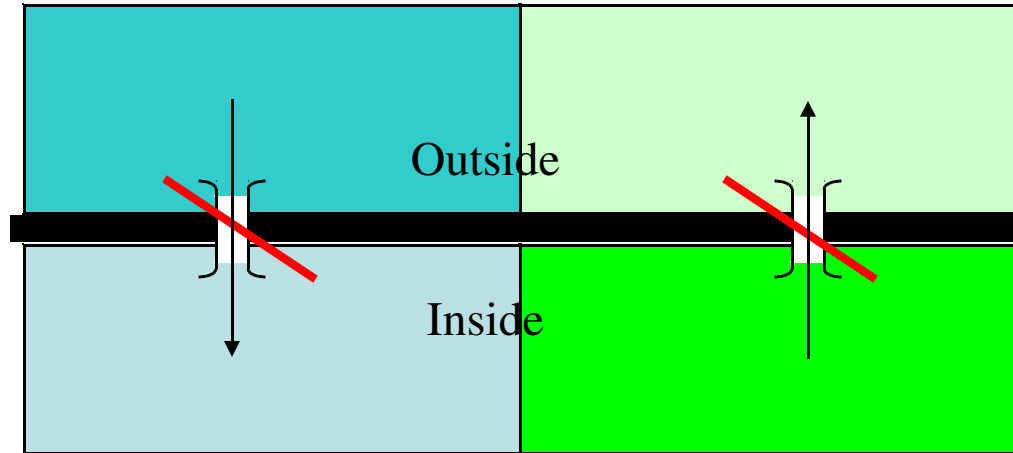
Nernst Equation: $E = (RT/z) \ln([\text{outside}]/[\text{inside}])$

Reversal Potential for Na^+ is around $+50 \text{ mV}$ (based on typical concentration gradients)

Note: Reversal potential **does not** depend upon *resistance*.

The Membrane: Membrane Potential

Case 1: Two types of Ions (Na⁺ and K⁺)



Equilibrium Potential : When opposing currents balance each other out (-70 mV).

Goldman Equation:

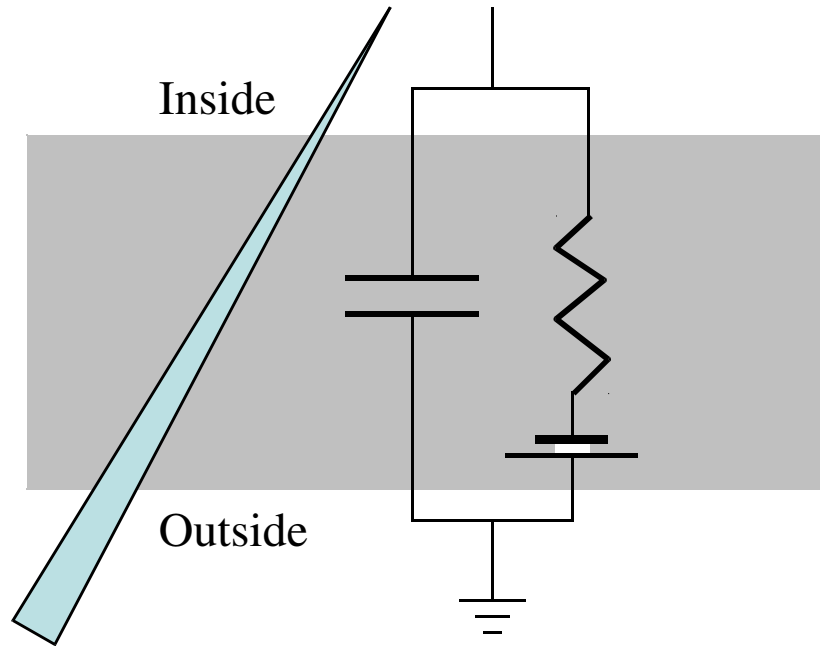
$$V = (-60\text{ mV}) * \log_{10} \left(\frac{P_K [K]_{in} + P_{Na} [Na]_{in} + P_{Cl} [Cl]_{out}}{P_K [K]_{out} + P_{Na} [Na]_{out} + P_{Cl} [Cl]_{in}} \right)$$

Note: Equilibrium potential **does** depend upon relative *resistances*.

Reversal potentials ---- Na⁺ : $+50\text{ mV}$ K⁺ : -80 mV

Neuroelectronics.org *Why ingesting Potassium Chloride is deadly; ingesting Sodium Chloride is not.*

Passive membrane: Equivalent Circuit



Voltage independent channels

Single Compartment

Electrotonically compact neuron.

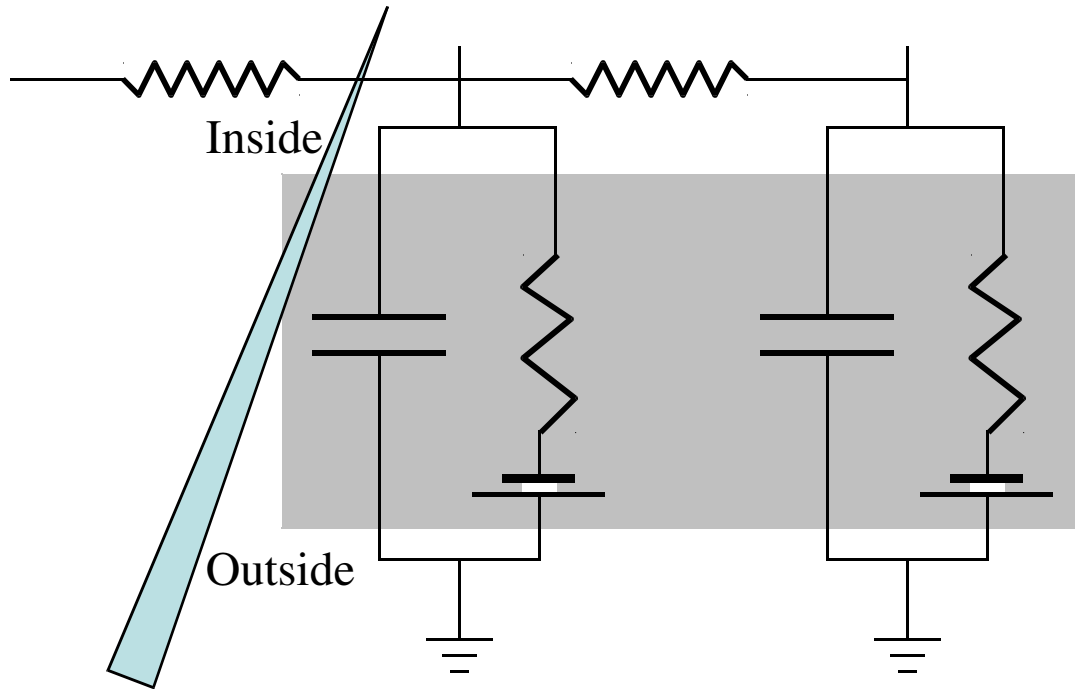
$$I_{INJ} = I$$

$$I = C \, dV/dt + (V - E_L)/R$$

Use new variable: $V = V - E_L$

$$(C * R) \, dV/dt = -V + IR$$

Passive membrane: Cable Equation



Voltage independent channels

Multiple Compartments

Electrotonically non-compact neuron.

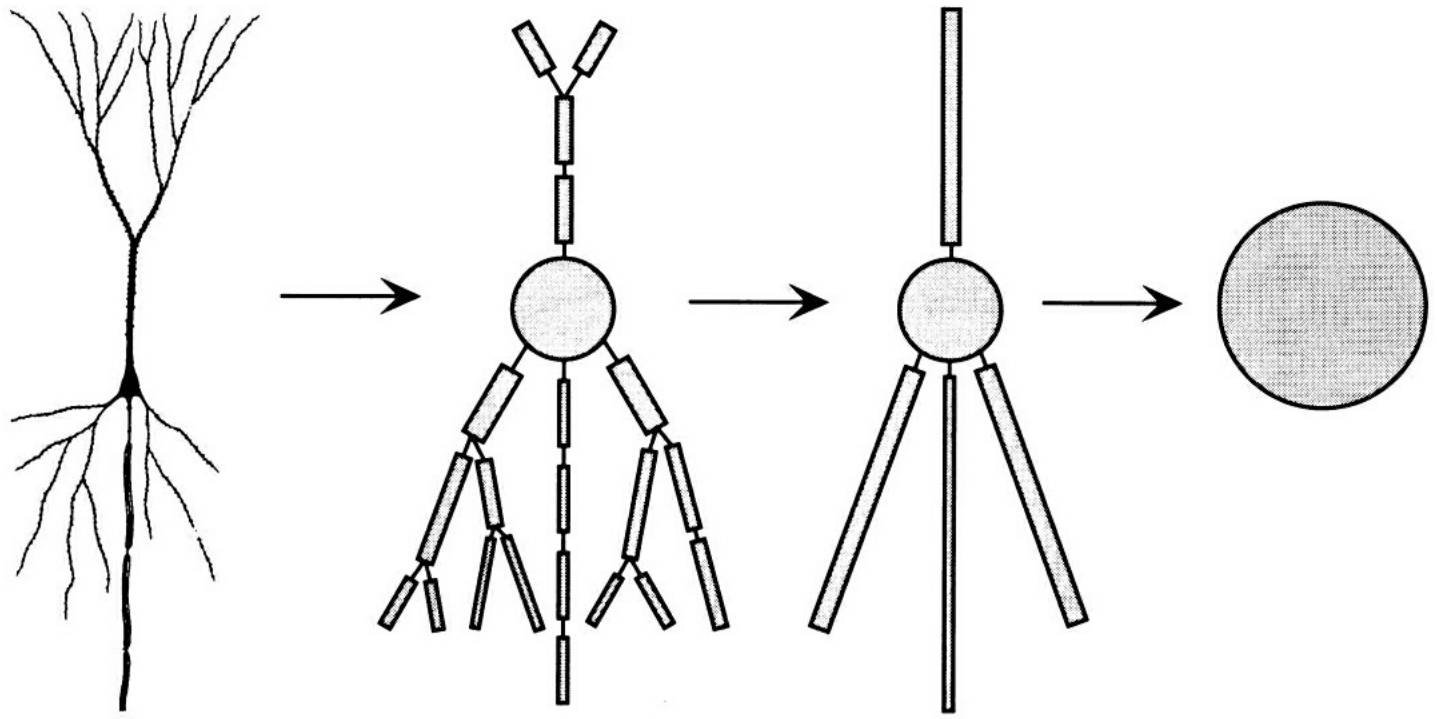
$$C \frac{\partial V}{\partial t} = -V/R + I$$

$$\frac{\partial V}{\partial x} = ir \quad \text{hence} \quad \frac{\partial^2 V}{\partial x^2} = r \frac{\partial i}{\partial x}$$

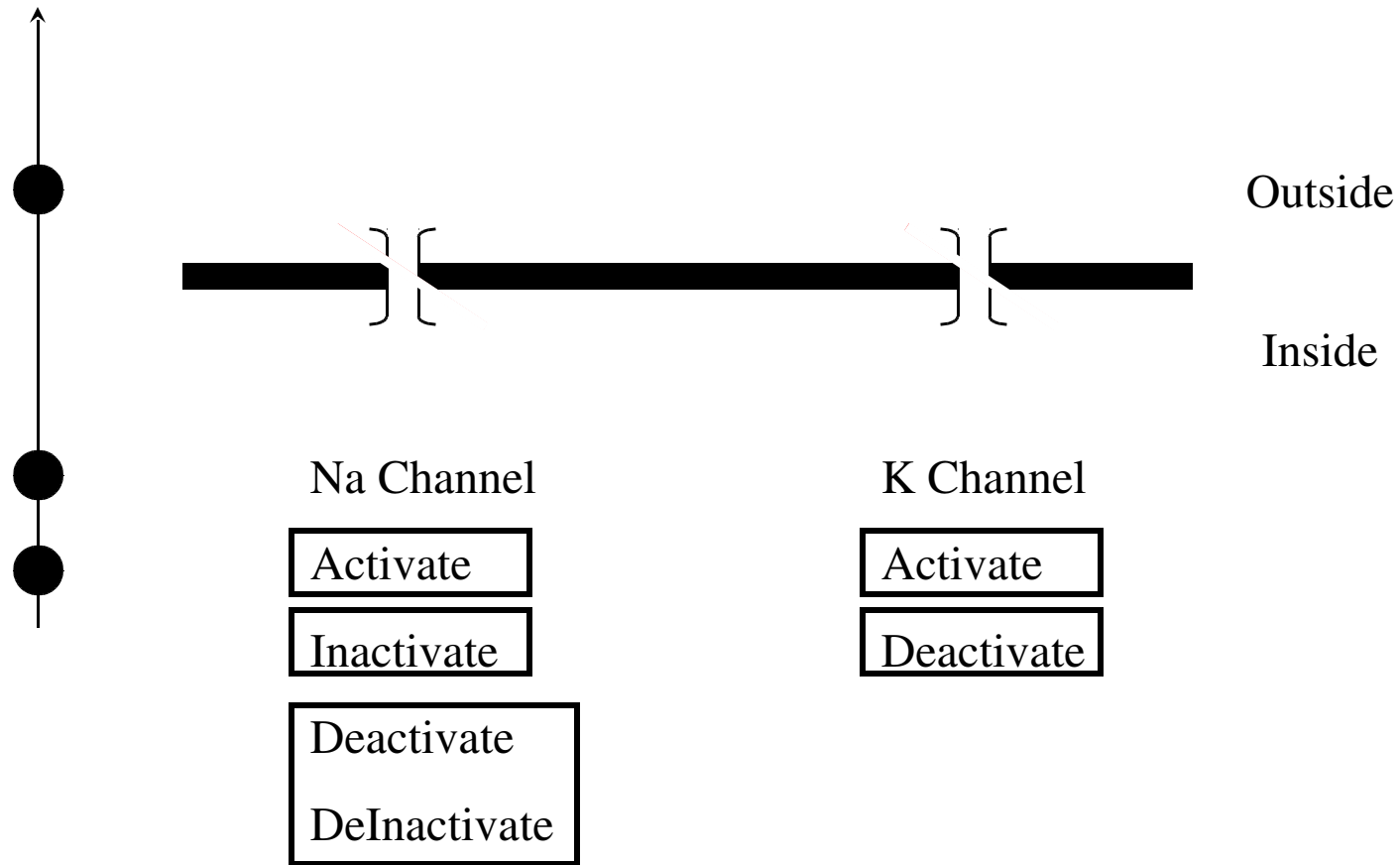
$$I_{\text{INJ}} = I - \frac{\partial i}{\partial x} \quad \text{hence} \quad I = I_{\text{INJ}} + \frac{\partial i}{\partial x}$$

$$C \frac{\partial V}{\partial t} = (1/r) \frac{\partial^2 V}{\partial x^2} - (1/R)V + I_{\text{INJ}}$$

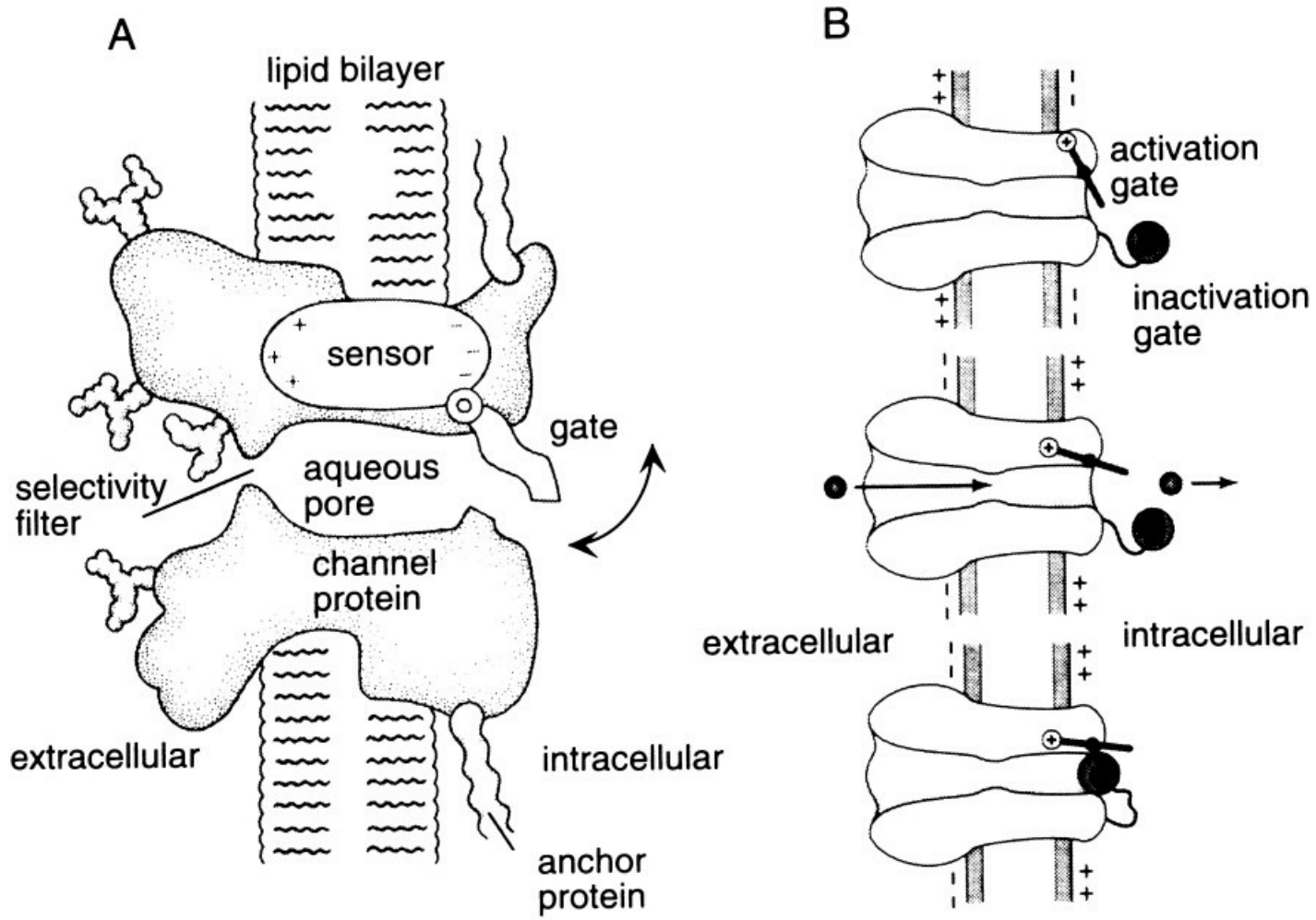
Passive membrane: Compartmental Model



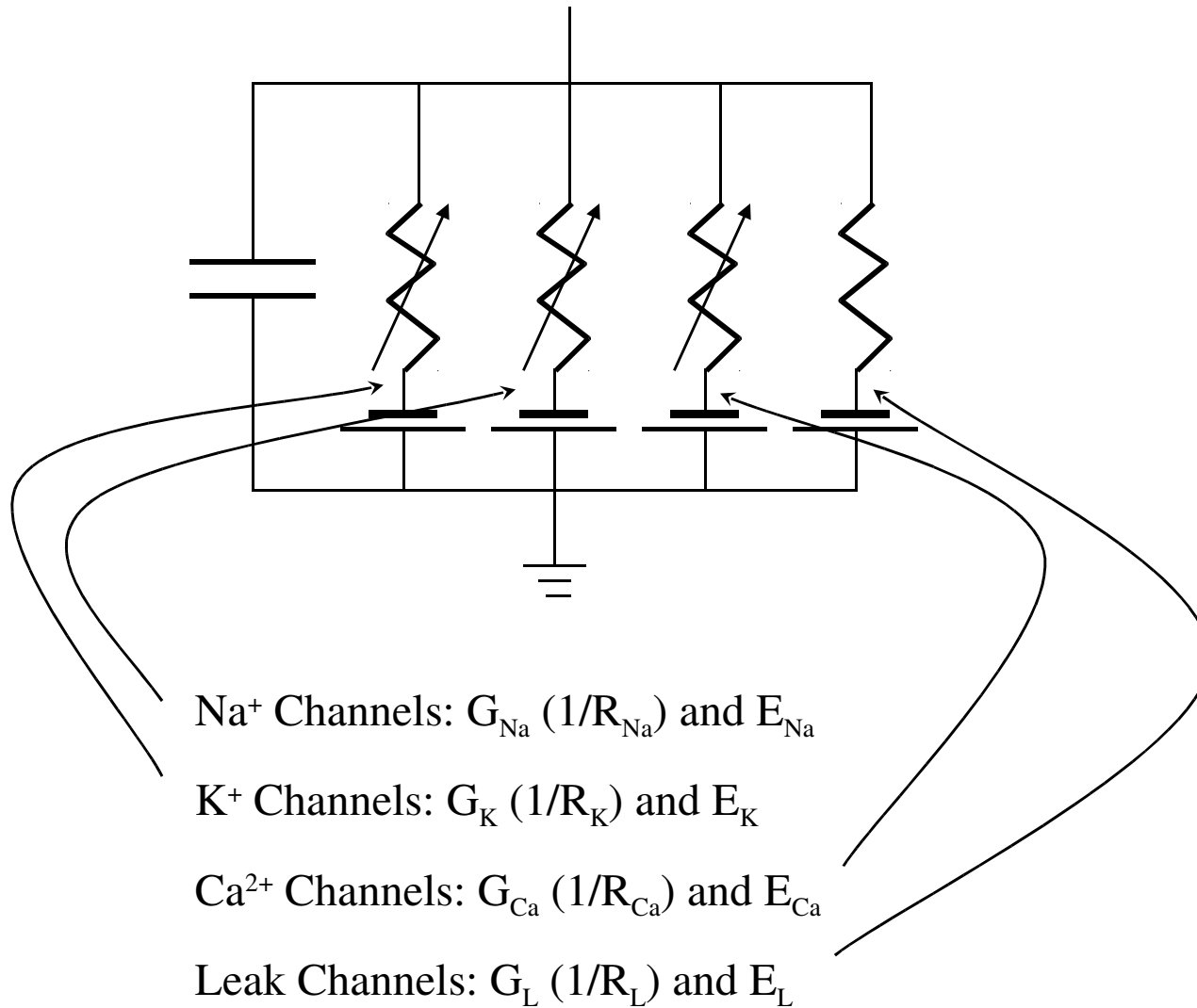
Active membrane: Voltage Dependent Conductance



Active membrane: Sodium Channel

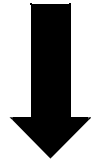


Active membrane: Voltage Dependent Conductance

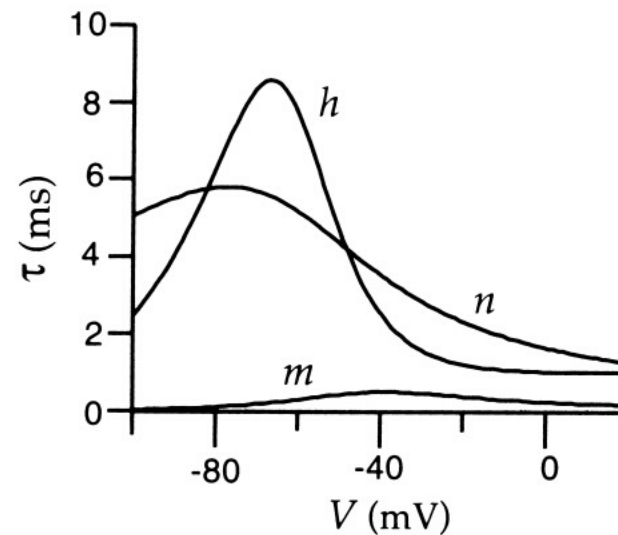
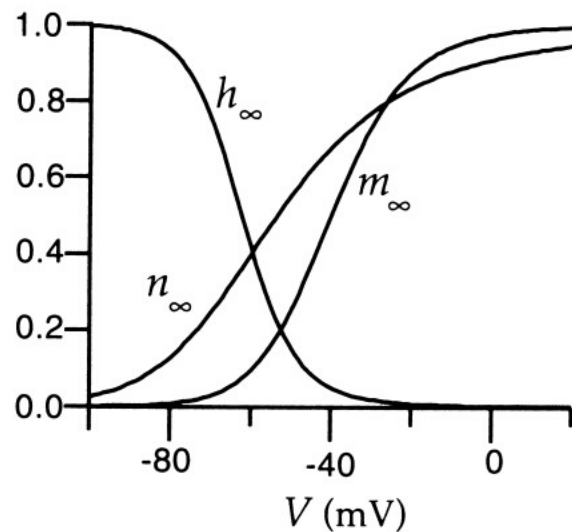


Active membrane: Hodgkin Huxley Equations

$$I = C \frac{dV}{dt} + G_L(V - E_L)$$



$$I = C \frac{dV}{dt} + G_L(V - E_L) + G_K n^4(V - E_K) + G_{Na} m^3 h(V - E_{Na})$$



Active membrane: Hodgkin Huxley Equations

$$dn/dt = a_n(V)(1-n) - b_n(V)n \quad a_n(V) = \text{opening rate} \quad b_n(V) = \text{closing rate}$$

$$dm/dt = a_m(V)(1-m) - b_m(V)m \quad a_m(V) = \text{opening rate} \quad b_m(V) = \text{closing rate}$$

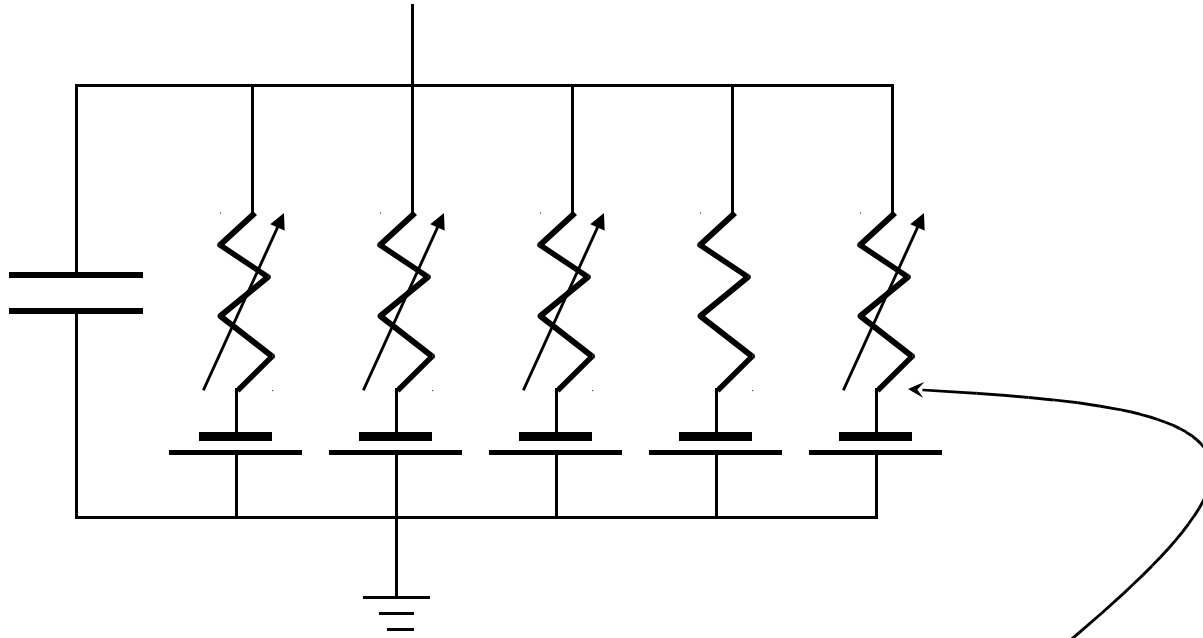
$$dh/dt = a_h(V)(1-h) - b_h(V)h \quad a_h(V) = \text{opening rate} \quad b_h(V) = \text{closing rate}$$

$$a_n = (0.01(V+55)) / (1 - \exp(-0.1(V+55))) \quad b_n = 0.125 \exp(-0.0125(V+65))$$

$$a_m = (0.1(V+40)) / (1 - \exp(-0.1(V+40))) \quad b_m = 4.00 \exp(-0.0556(V+65))$$

$$a_h = 0.07 \exp(-0.05(V+65)) \quad b_h = 1.0 / (1 + \exp(-0.1(V+35)))$$

Active membrane: Synaptic Conductance

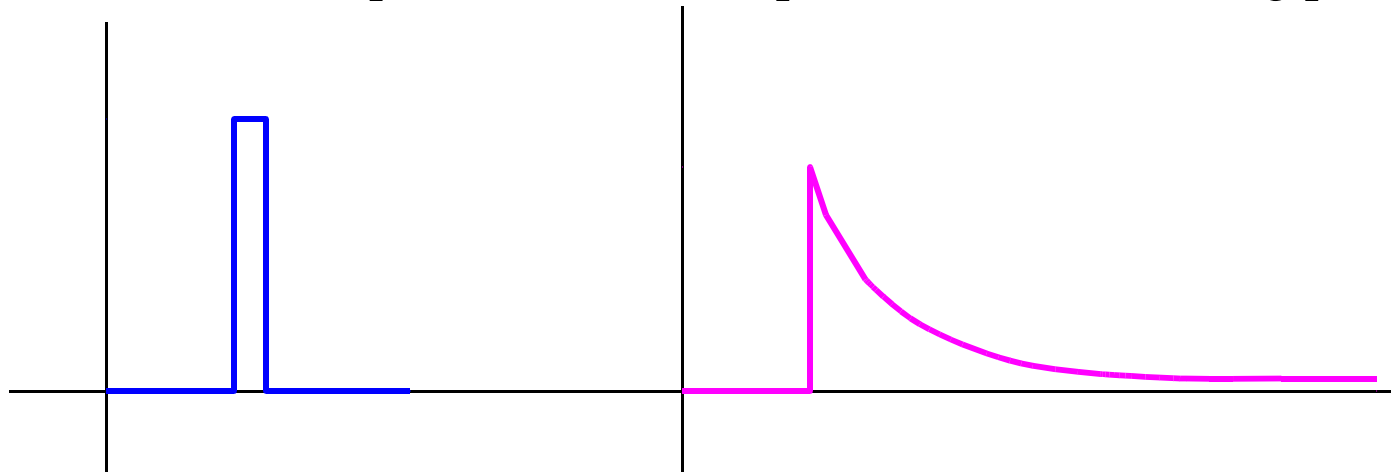


Synaptic Channels: G_{Syn} ($1/R_{\text{Syn}}$) and E_{Syn}

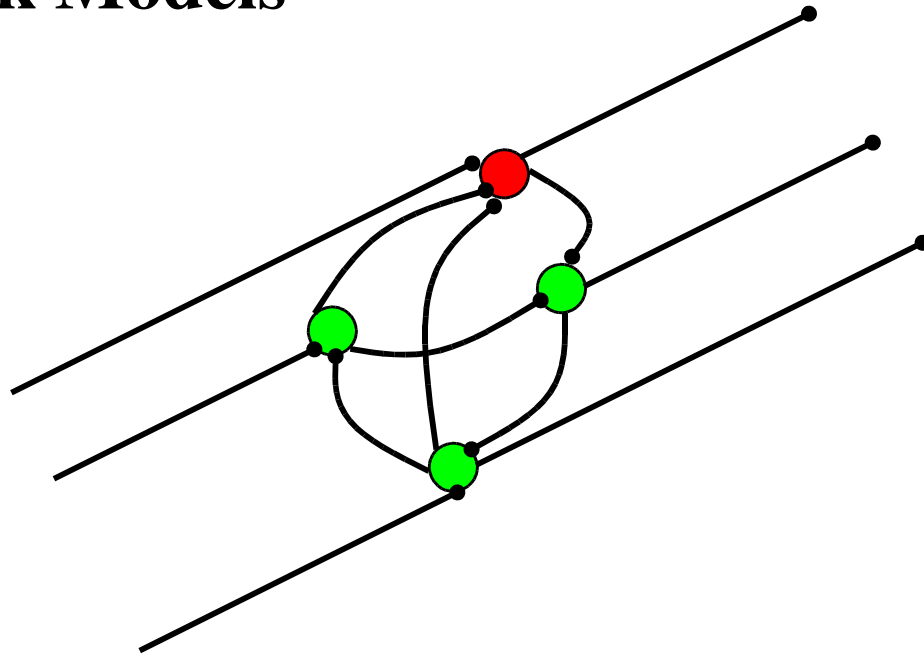
Reduced Model: Leaky Integrate and Fire

$$C dV/dt = -G_L(V - E_L) + I$$

- Assume that synaptic response is an injected current rather than a change in conductance.
- Assume injected current is a δ function; Results in PSP
- Linear System: Total effect at soma = sum of individual PSP's
- Neuron Spikes when total potential at soma crosses a threshold.
- Reset membrane potential to a reset potential (can be resting potential)



Network Models



Biggest Difficulty:

Spikes \rightarrow Membrane Potential \rightarrow Spikes

Membrane Potential \rightarrow Spikes \rightarrow Membrane Potential



Firing Rate Model

Exact spike sequence converted into instantaneous rate $r(t)$

Justification: Each neuron has large number of inputs which are generally not very **correlated**.

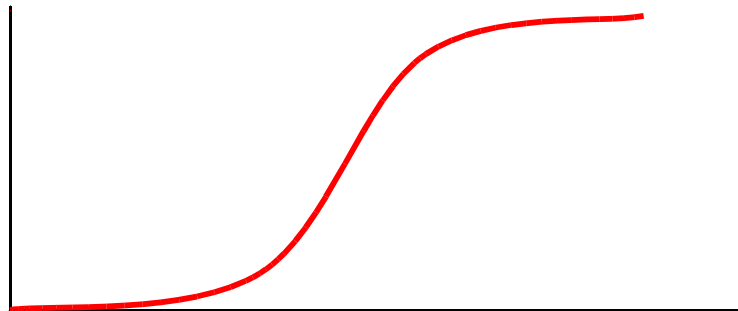
2 Steps:

Firing Rate of Presynaptic Neuron \rightarrow Synaptic Input to Postsynaptic Neurons

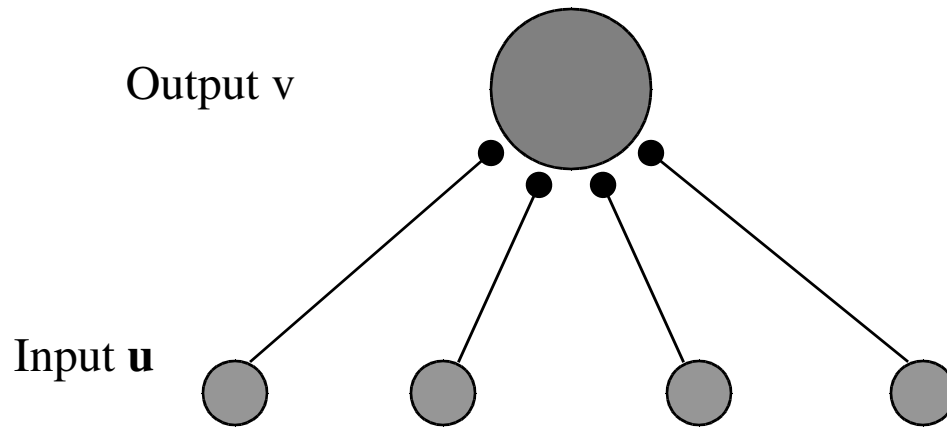
Total Input to Postsynaptic Neuron \rightarrow Firing rate of Postsynaptic Neuron

Total Synaptic Input modeled as total current injected into the soma

f-I curve: Output Spike Frequency vs. Injected Current curve



Firing Rate Model

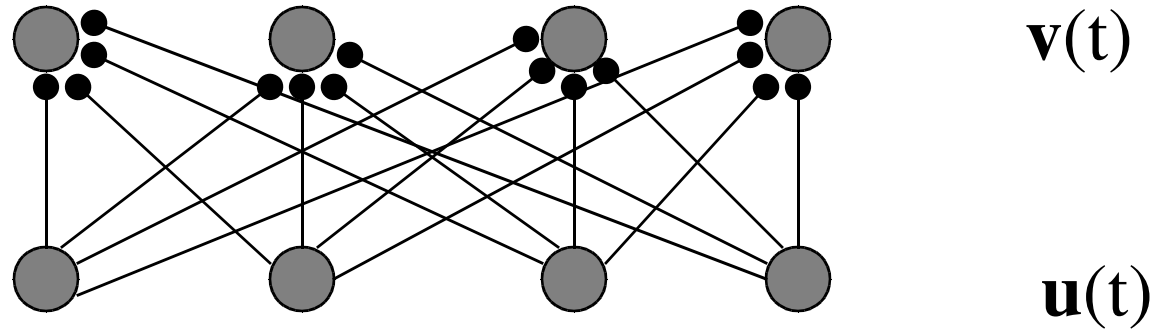


Firing rate does not follow changes in total synaptic current instantaneously, hence

$$\tau \frac{dv}{dt} = -v + F(I(t))$$

$$I(t) = \mathbf{w} \cdot \mathbf{u}(t)$$

Firing Rate Network Model



$$\tau \frac{d\mathbf{v}}{dt} = -\mathbf{v} + F(\mathbf{w} \cdot \mathbf{u}(t))$$